# Al-Powered Precision: Real-Time Markerless Tracking in X-Ray Imaging

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Memorial Sloan Kettering Cancer Center

### **Conflict of interest**

None

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### **Markerless lung tumor tracking**

- X-ray based
  - CyberKnife
  - Radixact Tomotherapy
  - RapidTrac (Varian, not FDA approved)

RADIXACT<sup>®</sup> SERIES





CyberKnife

### • MRI-LINAC

- □ Real-time 2D MR image in CINE mode (5 frames/sec)
- Superior soft tissue contrast
- Automatic gating system with soft tissue tracking
- □ Template-matching with Cross-correlation



Elekta Unity MR-LINAC with 1.5T MR scanner

### Challenges of x-ray based markerless tumor tracking

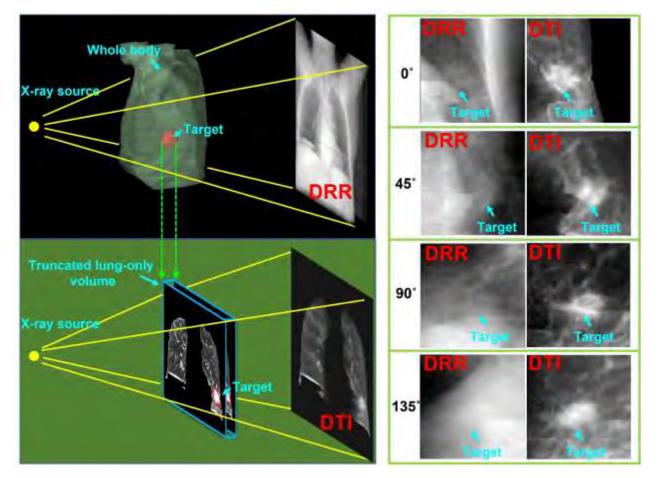
### Poor X-ray image quality

- Low tumor contrast
- □ Scatter, beam hardening and noise
- □ Superimposition of multiple structures

### Can we provide high-quality x-ray imaging to facilitate more accurate markerless lung tumor tracking on conventional LINAC platform?

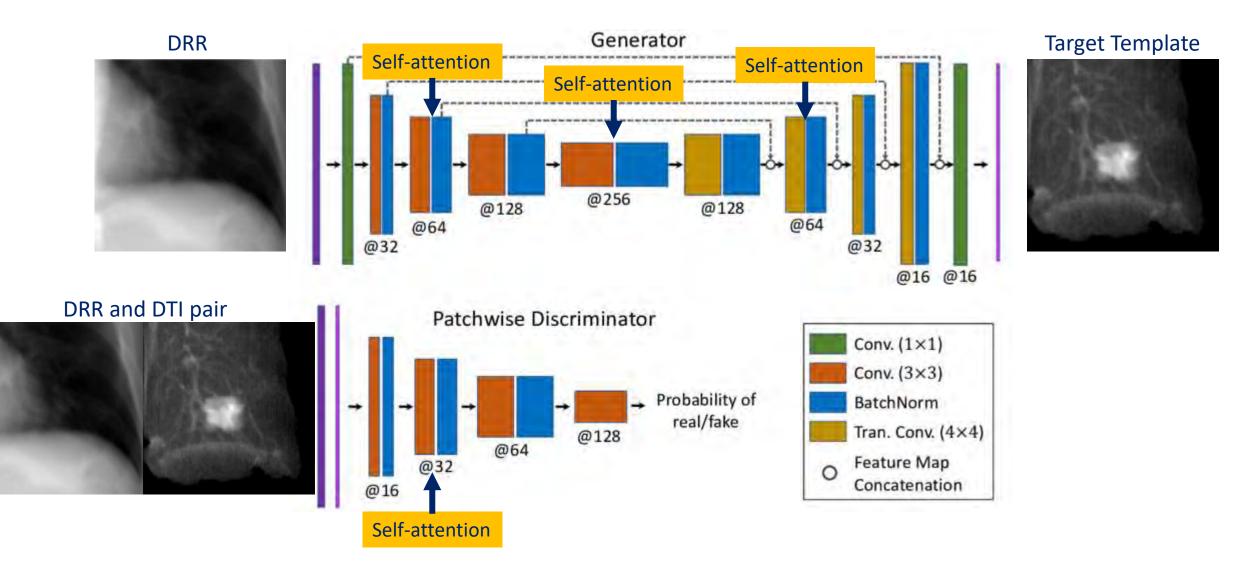
# Al-based target decomposition technique in on-board KV imaging

Decomposed target image (DTI)



Fu Y, et al, "Enhancing the target visibility with synthetic target specific digitally reconstructed radiograph for intrafraction motion monitoring: A proof-of-concept study. Med. Phys. 2023 50(12):7791-7805 © 2023 Memorial Sloan Kettering Cancer Center, et al. All rights reserved.

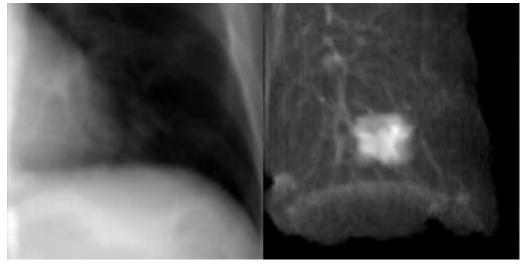
### Image Translation using cGAN with self-attention



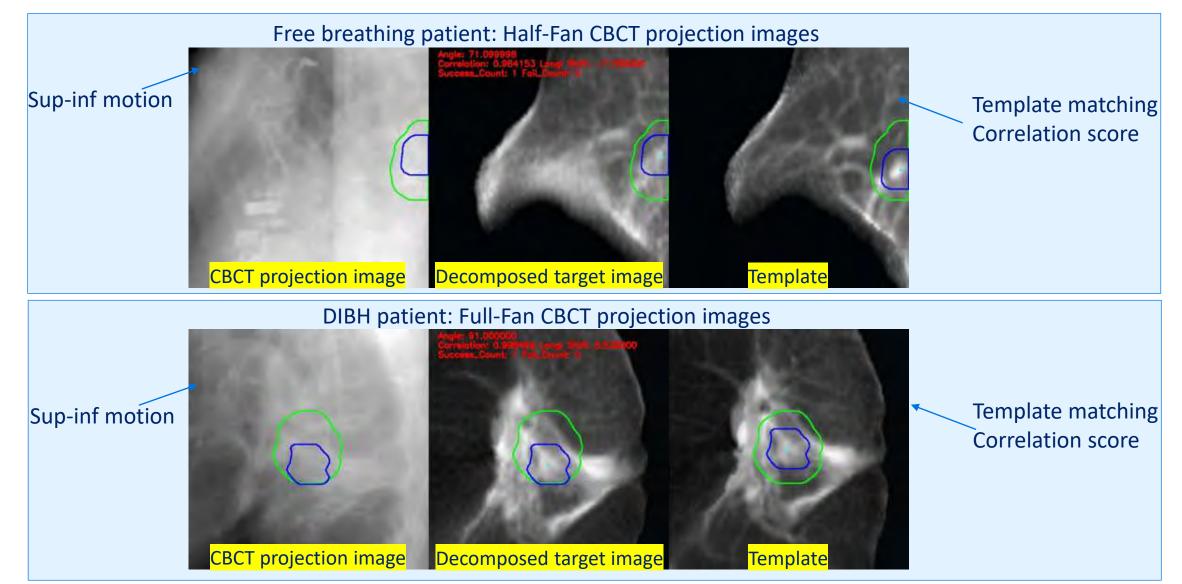
### **Patient-specific model**

- Training image generation
  4DCT, Free-breathing CT, DIBH CT
  DRR & DTI pair across 360-degree
  Augmentation by CT image translation
  # of images: 5000-20,000
- Model parameters
  - Generator: 55 M, Discriminator: 3 M
  - □ Speed: 6-12 hours for 200 epochs





### **Tumor tracking using template matching**



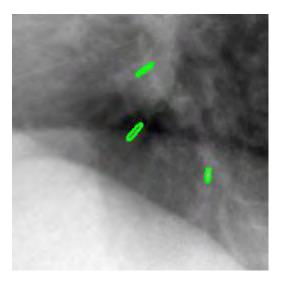
### **Tumor tracking validation**

• MSK 14-225 clinical protocol

Table 1. Tumor characteristics for the nine patients

• Tumor motion ground truth: beacon transponder trajectories in 2D

Subject	GTV Vol(cm <sup>3</sup> )	Equiv. Sphere Diam.(mm) of GTV	DTW(mm)	DTB(mm)	Max SI beacor motion (mm)
Pt 1	1.4	14	30	12	9.1
Pt 2	2.4	17	23	15	4.5
Pt 3	5.2	22	50	28	6.4
Pt 4	0.3	8	53	24	7.4
Pt 5	15.6	31	46	25	20.4
Pt 6	107.7	59	33	30	14.6
Pt 7	9.4	26	20	22	6.2
Pt 8	4.8	21	45	13	11.4
Pt 9	6.58	23	24	17	19.0



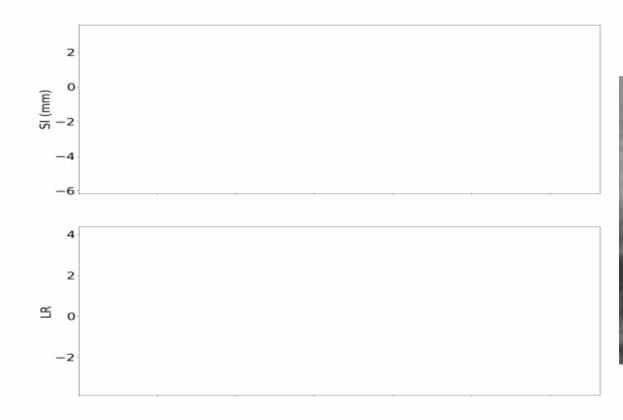
Note: GTV is the gross tumor volume, delineated on the planning CT. DTW is the distance between the tumor and the thorax wall. DTB is the distance between the tumor and the nearest implanted beacon transponder.

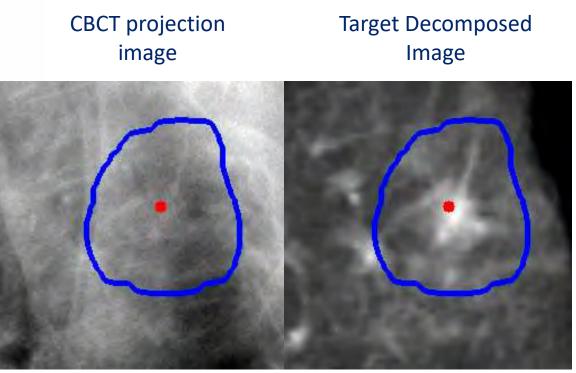
#### MSK-14-225 clinical protocol:

Investigation of Respiratory Motion-Corrected Cone-Beam CT and Intratreatment Gating Based on Electromagnetic Transponders to Reduce Target Position Uncertainty in Radiation Treatment of Lung Malignancies

### **Tumor tracking validation**

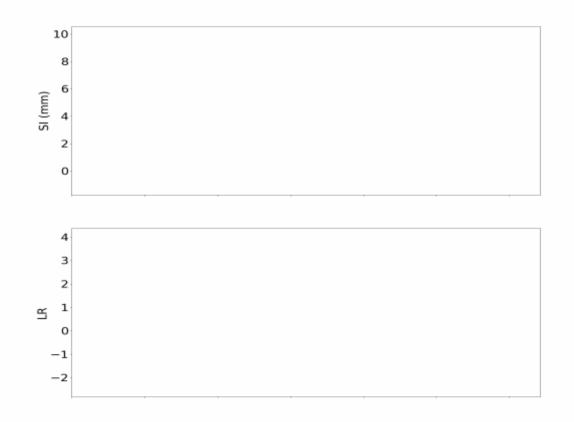
- Beacon trajectory in red curve
- Our tracking trajectory is in blue curve

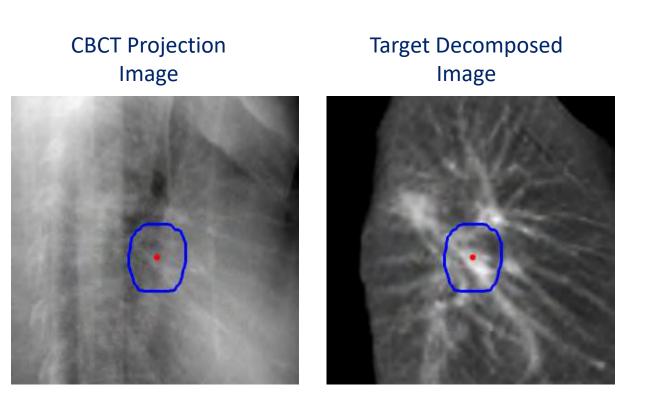




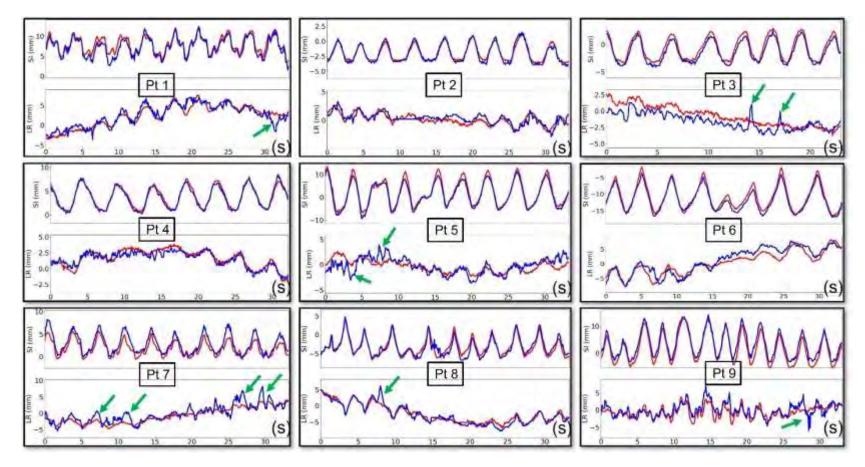
### **Tumor tracking validation**

- Beacon trajectory in red curve
- Our tracking trajectory is in blue curve





# Tumor tracking verification using Calypso beacon transponder trajectories



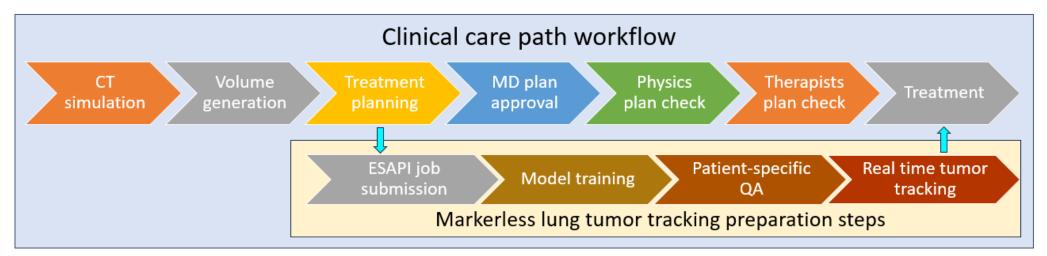
2D tumor trajectories of the beacon transponders (red) and the template matching results (blue) for the nine patients. Green arrows highlight the discrepancies between the red and the blue trajectories.

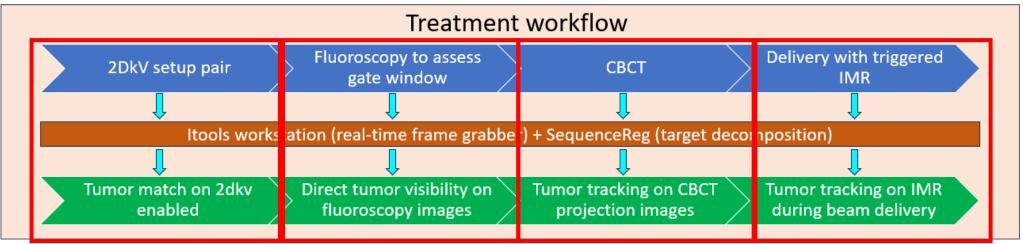
### **Tumor tracking results comparison**

	results are shown			<b>D</b> 1 D		B: E	<b>D</b> : <i>C</i>		<b>D</b> : 0		
	Subject	Pt 1	Pt 2	Pt 3	Pt 4	Pt 5	Pt 6	Pt 7	Pt 8	Pt 9	Avg
	AME (SI)	0.7±0.6	0.3±0.2	0.7±0.3	0.3±0.3	1.0±0.8	0.9±0.6	1.1±0.7		1.7±0.9	0.8±0.7
Proposed	AME (IPLR)	0.8±0.8	0.5±0.4	1.0±0.6	0.4±0.3	0.9±0.8	1.5±1.0	1.1±0.9		1.1±1.0	0.9±0.8
•	90 Perc. (SI)	1.6	0.5	1.1	0.6	2.1	1.6	1.9		2.8	1.5
(template matching on DTI)	90 Perc. (IPLR)	1.7	1.0	1.8	0.9	2.2	2.7	2.3		2.3	1.8
	Traj. Corr (SI)	0.93	0.98	0.99	0.98	0.99	0.99	0.95		0.98	0.97±0.03
	Traj. Corr (IPLR)	0.92	0.79	0.84	0.93	0.60	0.93	0.89		0.69	0.84±0.11
	TR (SI < 5mm)	100.0%	100.0%	100.0%	100.0%	100.0%	100.0%	100.0%		99.8%	100.0%
	TR (SI<2mm) TR (IPLR<2mm)	94.6% 93.0%	100.0% 100%	<b>100.0%</b> 92.8%	100.0% 100%	<b>87.4%</b> 88.2%	96.6% 70.9%	90.5% 86.9%		64.1% 84.9%	92.2%
	TR(SI&IPLR<2mm)	93.0% 87.8%	100%	92.8%	100%	78.8%	69.1%	81.5%		57.1%	84.6%
	Note: 90 Perc. is the	e 90 percer	ntile. Traj. (	Corr is the t	trajectory (	correlation	coefficien	t. TR is the	successful	tracking r	ate.
	Table 3. Absolute correlation coeff	e mean er icients in	ror (AME) the SI an	) in mm u d IPLR dir	sing the c	original kV	projectio	on images	s, 90 perce	entile in r	nm, trajecto
	Table 3. Absolute correlation coeff	e mean er icients in	ror (AME) the SI an	) in mm u d IPLR dir	sing the c	original kV	projectio	on images	s, 90 perce	entile in r	nm, trajecto
	Table 3. Absolute correlation coeff Table 2, better re	e mean er icients in sults are s	ror (AME) the SI an shown in	) in mm u d IPLR dir bold.	sing the c	original kV and succe	projectic ssful trac	on images king rate	, 90 perce for the 9	entile in r patients	mm, trajecto . Compared
Comparison	Table 3. Absolute correlation coeff Table 2, better re Subject	e mean er icients in esults are : <b>Pt 1</b>	ror (AME) the SI an shown in <b>Pt 2</b>	) in mm u d IPLR dir bold. <b>Pt 3</b>	sing the c rections, a Pt 4	original kV and succe <b>Pt 5</b>	' projectio ssful trac <b>Pt 6</b>	on images king rate <b>Pt 7</b>	5, 90 perce for the 9 <b>Pt 8</b>	entile in r patients Pt 9	mm, trajecto . Compared <b>Avg</b> 1.5±1.9
Comparison	Table 3. Absolute correlation coeff Table 2, better re Subject AME (SI)	e mean er icients in esults are Pt 1 1.5±1.4	ror (AME) the SI an shown in <b>Pt 2</b> 0.4±0.3	) in mm u d IPLR dir bold. <b>Pt 3</b> 0.9±0.6	sing the c rections, a <b>Pt 4</b> 0.4±0.4	original kV and succe <b>Pt 5</b> 2.4±2.5	r projection ssful trac <b>Pt 6</b> 1.1±1.5	on images king rate <b>Pt 7</b> 2.2±1.5	5, 90 perce for the 9 <b>Pt 8</b> 1.1±1.6	entile in r patients <b>Pt 9</b> 3.1±2.9	mm, trajecto . Compared <b>Avg</b> 1.5±1.9
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method	Table 3. Absolute correlation coeff Table 2, better re Subject AME (SI) AME (IPLR) 90 Perc. (SI)	e mean er icients in esults are s <b>Pt 1</b> 1.5±1.4 2.3±1.6 3.8	ror (AME) the SI an shown in Pt 2 0.4±0.3 0.5±0.4 0.7	) in mm u d IPLR dir bold. <b>Pt 3</b> 0.9±0.6 <b>0.7±0.4</b> 1.6	sing the c rections, a <b>Pt 4</b> 0.4±0.4 0.5±0.4 1.0	Priginal kV and succe Pt 5 2.4±2.5 1.0±0.7 5.4	projectic ssful trac <b>Pt 6</b> 1.1±1.5 3.4±3.0 1.9	on images king rate <b>Pt 7</b> 2.2±1.5 1.2±0.9 4.4	5, 90 perce for the 9 Pt 8 1.1±1.6 0.7±0.5 2.7	entile in r patients <b>Pt 9</b> 3.1±2.9 1.6±2.0 7.5	mm, trajecto . Compared Avg 1.5±1.9 1.4±1.7 3.4
	Table 3. Absolute correlation coeff Table 2, better re Subject AME (SI) AME (IPLR) 90 Perc. (SI) 90 Perc. (IPLR)	e mean er icients in esults are e Pt 1 1.5±1.4 2.3±1.6 3.8 4.6	ror (AME) the SI an shown in Pt 2 0.4±0.3 0.5±0.4 0.7 1.0	) in mm u d IPLR dir bold. <b>Pt 3</b> 0.9±0.6 <b>0.7±0.4</b> 1.6 <b>1.2</b>	sing the c rections, a <b>Pt 4</b> 0.4±0.4 0.5±0.4 1.0 1.0	Priginal kV and succe Pt 5 2.4±2.5 1.0±0.7 5.4 1.9	r projections ssful trac Pt 6 1.1±1.5 3.4±3.0 1.9 9.0	on images king rate Pt 7 2.2±1.5 1.2±0.9 4.4 2.5	5, 90 perce for the 9 Pt 8 1.1±1.6 0.7±0.5 2.7 1.4	entile in r patients Pt 9 3.1±2.9 1.6±2.0 7.5 4.1	mm, trajecto . Compared <b>Avg</b> 1.5±1.9 1.4±1.7 3.4 3.1
method (Template matching on	Table 3. Absolute correlation coeff Table 2, better re Subject AME (SI) AME (IPLR) 90 Perc. (SI) 90 Perc. (IPLR) Traj. Corr (SI)	e mean er icients in esults are s Pt 1 1.5±1.4 2.3±1.6 3.8 4.6 0.54	ror (AME) the SI an shown in Pt 2 0.4±0.3 0.5±0.4 0.7 1.0 0.98	) in mm u d IPLR dir bold. <b>Pt 3</b> 0.9±0.6 <b>0.7±0.4</b> 1.6 <b>1.2</b> 0.96	sing the c rections, a <b>Pt 4</b> 0.4±0.4 0.5±0.4 1.0 1.0 0.96	Priginal kV and succe Pt 5 2.4±2.5 1.0±0.7 5.4 1.9 0.89	<sup>7</sup> projectic ssful trac <b>Pt 6</b> 1.1±1.5 3.4±3.0 1.9 9.0 0.88	on images king rate Pt 7 2.2±1.5 1.2±0.9 4.4 2.5 0.76	5, 90 perce for the 9 <b>Pt 8</b> 1.1±1.6 <b>0.7±0.5</b> 2.7 1.4 0.98	entile in r patients <b>Pt 9</b> 3.1±2.9 1.6±2.0 7.5 4.1 0.27	mm, trajecto . Compared <b>Avg</b> 1.5±1.9 1.4±1.7 3.4 3.1 0.80±0.16
method	Table 3. Absolute correlation coeff Table 2, better re Subject AME (SI) AME (IPLR) 90 Perc. (SI) 90 Perc. (IPLR) Traj. Corr (SI) Traj. Corr (IPLR)	e mean er icients in esults are s Pt 1 1.5±1.4 2.3±1.6 3.8 4.6 0.54 0.82	ror (AME) the SI an shown in Pt 2 0.4±0.3 0.5±0.4 0.7 1.0 0.98 0.61	) in mm u d IPLR dir bold. <b>Pt 3</b> 0.9±0.6 <b>0.7±0.4</b> 1.6 <b>1.2</b> 0.96 <b>0.95</b>	sing the c rections, a <b>Pt 4</b> 0.4±0.4 0.5±0.4 1.0 1.0 0.96 0.89	Priginal kV      and succe      Pt 5      2.4±2.5      1.0±0.7      5.4      1.9      0.89      0.74	projectic ssful trac <b>Pt 6</b> 1.1±1.5 3.4±3.0 1.9 9.0 0.88 0.65	on images king rate <b>Pt 7</b> 2.2±1.5 1.2±0.9 4.4 2.5 0.76 0.77	5, 90 perce for the 9 <b>Pt 8</b> 1.1±1.6 <b>0.7±0.5</b> 2.7 1.4 0.98 0.77	entile in r patients <b>Pt 9</b> 3.1±2.9 1.6±2.0 7.5 4.1 0.27 0.39	mm, trajecto . Compared <b>Avg</b> 1.5±1.9 1.4±1.7 3.4 3.1 0.80±0.16 0.76±0.22
<b>method</b> (Template matching on	Table 3. Absolute correlation coeff Table 2, better re Subject AME (SI) AME (IPLR) 90 Perc. (SI) 90 Perc. (IPLR) Traj. Corr (SI) Traj. Corr (IPLR) TR (SI < 5mm)	e mean er icients in esults are s Pt 1 1.5±1.4 2.3±1.6 3.8 4.6 0.54 0.82 96.0%	ror (AME) the SI an shown in Pt 2 0.4±0.3 0.5±0.4 0.7 1.0 0.98 0.61 100.0%	) in mm u d IPLR dir bold. <b>Pt 3</b> 0.9±0.6 <b>0.7±0.4</b> 1.6 <b>1.2</b> 0.96 <b>0.95</b> 100.0%	sing the c rections, a <b>Pt 4</b> 0.4±0.4 0.5±0.4 1.0 1.0 0.96 0.89 100.0%	Priginal kV and succe Pt 5 2.4±2.5 1.0±0.7 5.4 1.9 0.89 0.74 100.0%	<sup>7</sup> projectic ssful trac <b>Pt 6</b> 1.1±1.5 3.4±3.0 1.9 9.0 0.88 0.65 95.6%	on images king rate Pt 7 2.2±1.5 1.2±0.9 4.4 2.5 0.76 0.77 94.8%	5, 90 perce for the 9 <b>Pt 8</b> 1.1±1.6 <b>0.7±0.5</b> 2.7 1.4 0.98 0.77 93.6%	Pt 9 3.1±2.9 1.6±2.0 7.5 4.1 0.27 0.39 78.0%	mm, trajecto . Compared 1.5±1.9 1.4±1.7 3.4 3.1 0.80±0.16 0.76±0.22 94.7%

### **Clinical workflow**

• Model training triggered by the planner using ESAPI scripts



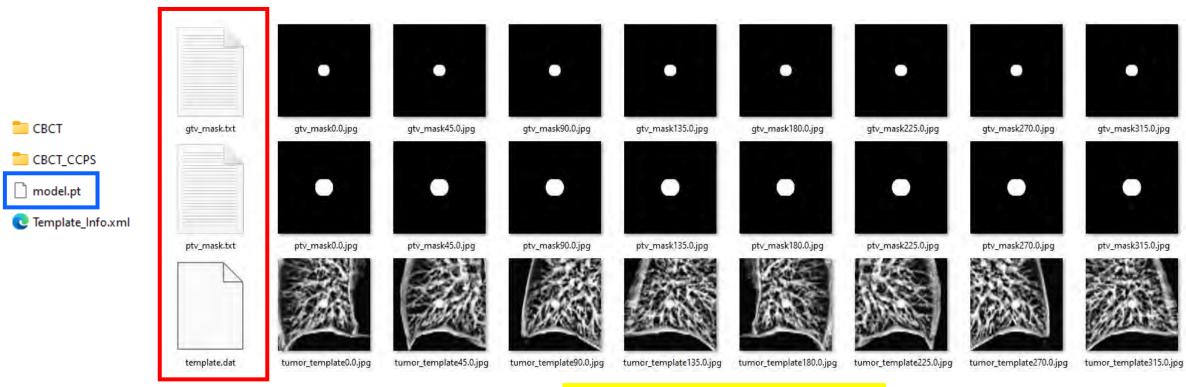


• Model training triggered by the planner using ESAPI scripts

e: FB:z_Lun			Cincentry Proves	chinterior 🐃 (	and an arrange				late: DIBH:z		1	Currenter Party	chInterior Couch_surfa	
Label	ст	ls	planning CT	Check Struct	ture	-	1	Temp	Label	СТ	2	s planning CT	Check Structure	
FB	CT_LUNGFB_030824	*		z_Lungs	*				DIBH_1					
4DCT_00%	CT_00	*		z_Lungs	*				DIBH_2		*		~	
4DCT_10%	CT_10	×		z_Lungs	*				DIBH_3		*		8	
4DCT_20%	CT_20	~		z_Lungs	*	-				- A.				
4DCT_30%	CT_30	÷		z_Lungs	*									
4DCT_40%	CT_40	~		z_Lungs	~									
4DCT_50%	CT_50	*		z_Lungs	*									
4DCT_60%	CT_60	ч		z_Lungs										
4DCT_70%	CT_70	+		z_Lungs	*									
4DCT_80%	CT_80	~		z_Lungs	~									
4DCT_90%	CT_90	*		z_Lungs	*									

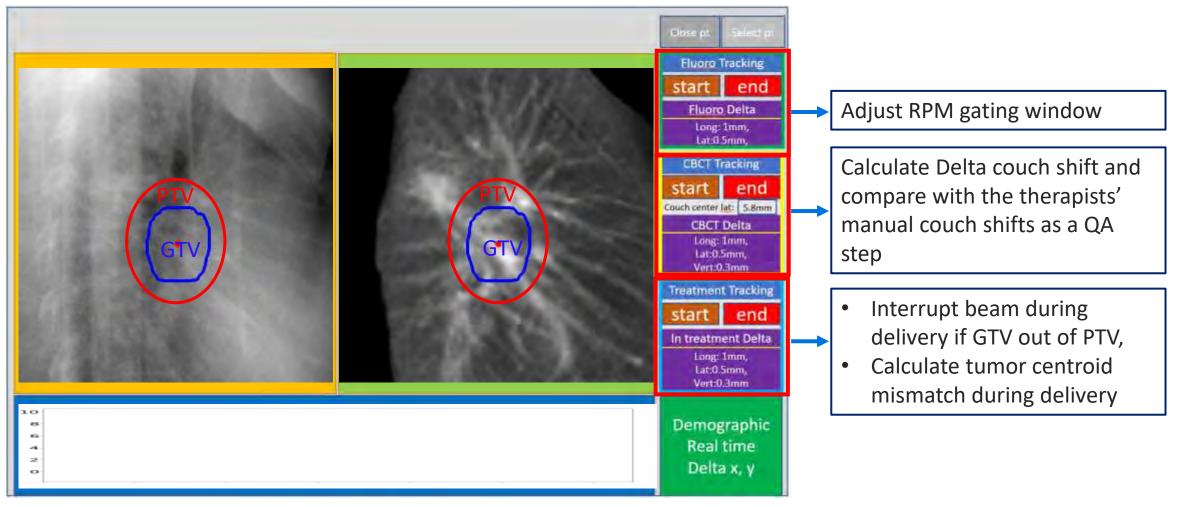
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• Model trained by high performance cluster



Target contour and template files

• GUI demo of the tracking software (under development)



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• QA phantom prototype with known tumor motion trace



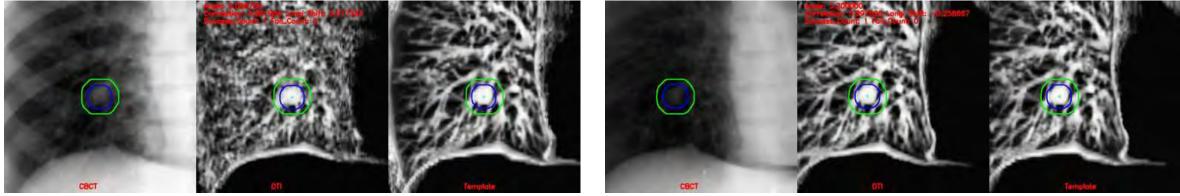
## **Clinical translation**

	Calc Couch Delta				True	Couch	n Delta		Error (mm)			
IMR during beam on	0.4	0.1	0		0	0	0		0.4	0.1	0	
spotlight CBCT	0.33	0.13	0		0	0	0	0.	.33	0.13	0	
full CBCT	-2	-0.24	-0.66		-2	-0.3	-0.3		0	0.06	0.36	
fluoro		0.5	-0.25			0			0	0.5	0.25	
	Vert	: Long	Lat		Vert	Long	Lat	Ver	t	Long	Lat	

• QA phantom tracking (static DIBH )

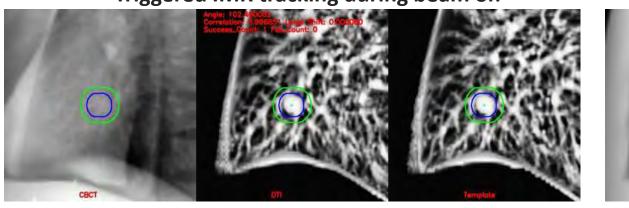
AP Fluoro



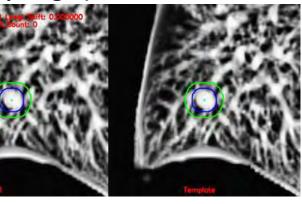


CBCI

#### Triggered IMR tracking during beam on



**CBCT (Spotlight)** 



### Conclusion

- AI-based target decomposition technique can provide high-quality x-ray imaging by removing unwanted overlapping structures and highlighting the target of interest on KV projection images.
- Real-time markerless lung motion monitoring is feasible on a conventional Linac platform.

### **Future works**

- Further improve the accuracy and robustness of the target decomposition technique by incorporating the DL-enhanced data augmentation strategy.
- Investigate a population-based model with fast patient-specific fine-tuning for scalability

### **Research Team**

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# Thank you for your attention!

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